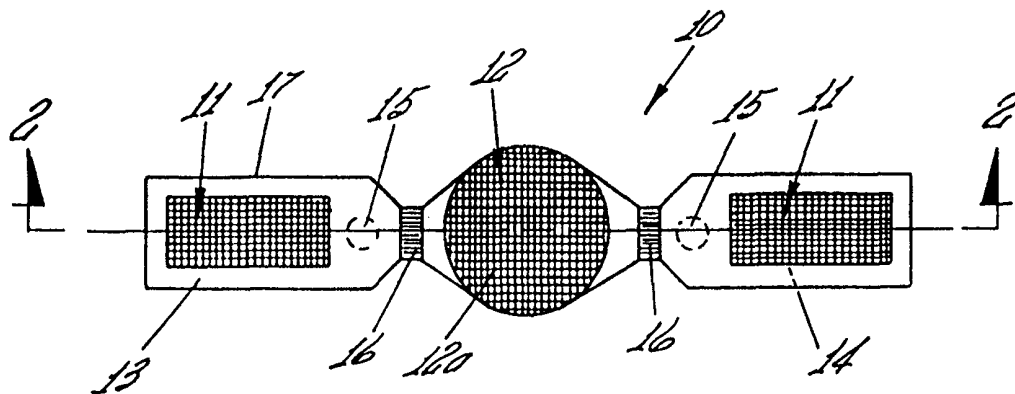


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(54) Title: IONTOPHORETIC DRUG DELIVERY ELECTRODES



(57) Abstract

Non-reusable, medicament-dispensing applicator electrodes (10) adapted for use with an iontophoresis device or an ionosonic device for facilitating delivery of medication across the cutaneous membrane into adjacent underlying tissues, and blood vessels. The embodiments of the iontophoresis electrode include an open mesh (12) having cells (12a) in the medicament dispensing portions (11) of the electrode which retain a medicament in the form of liquid, gel or ointment. The cells are adapted to contain, to iontophoretically dispense, and deliver medicament. The medicament-dispensing electrodes (70) are composite or unitary in construction and may be useful in the treatment of acne, and also genital herpes simplex infection. The delivery electrode (71), when used in accordance with the medicated electrode, and method described herein, demonstrated >90 % treatment efficacy in clinical trials for the treatment of genital herpes. The applicator electrode may also be used with an ionosonic handpiece (40).

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1
2 **TITLE: IONTOPHORETIC DRUG DELIVERY ELECTRODES**

3
4 **INVENTOR: JULIAN L. HENLEY, M.D.**

5
6 **SPECIFICATION**

7
8 **BACKGROUND OF THE INVENTION**

9
10 1. **Field of the Invention:**

11 This invention relates generally to the transdermal electrokinetic mass transfer
12 of medication into a diseased tissue, and, more specifically, to a iontophoresis
13 electrode for the transdermal delivery of medication into diseased tissues and blood
14 vessels adjacent to the delivery site.

15 2. **Prior Art:**

16 Iontophoresis has been employed for several centuries as a means for applying
17 medication locally through a patient's skin and for delivering medicaments to the eyes
18 and ears. The application of an electric field to the skin is known to greatly enhance
19 the skin's permeability to various ionic agents. This permeability change has been
20 used, for example, to enhance transcutaneous transport of glucose for monitoring
21 blood glucose levels. The use of iontophoretic transdermal delivery techniques has
22 obviated the need for hypodermic injection for many medicaments, thereby eliminating
23 the concomitant problems of trauma, pain and risk of infection to the patient.

24 Iontophoresis involves the application of an electromotive force to drive
25 charged ions into the dermal layers comprising or overlying a target tissue.
26 Particularly suitable target tissue includes tissues adjacent to the delivery site for
27 localized treatment or tissues remote therefrom in which case the medicament enters
28 into the circulatory system and is transported to a tissue by the blood. Positively
29 charged ions are driven into the skin at an anode while negatively charged ions are
30 driven into the skin at a cathode. Studies have shown increased skin penetration of

-2-

1 drugs at anodic or cathodic electrodes regardless of the predominant molecular ionic
2 charge on the drug. This effect is mediated by polarization and osmotic effects.

3 Regardless of the charge of the medicament to be administered, a
4 iontophoretic delivery device employs two electrodes (an anode and a cathode) in
5 conjunction with the patient's skin to form a closed circuit between one of the
6 electrodes (referred to herein alternatively as a "working" or "application" or
7 "applicator" electrode) which is positioned at the site of drug delivery and a passive or
8 "grounding" electrode affixed to a second site on the skin to enhance the rate of
9 penetration of the medicament into the skin adjacent to the applicator electrode.
10 Ultrasonic vibrations may be used in conjunction with iontophoresis to facilitate
11 iontophoretic deliver of a drug. An apparatus employing both iontophoresis and
12 ultrasonic vibrations to transdermally deliver medicament is referred to herein as an
13 ionosonic apparatus.

14 Recent interest in the use of iontophoresis for the transdermal delivery of
15 drugs to a desired cutaneous or subcutaneous treatment site has stimulated a redesign
16 of many of such drugs with concomitant increased efficacy of the drugs when
17 delivered transdermally. As iontophoretic delivery of medicaments become more
18 widely used, the opportunity for a consumer/patient to iontophoretically self-
19 administer a transdermal dosage of medicaments simply and safely at non-medical or
20 non-professional facilities would be desirable and practical. Similarly, when a
21 consumer/patient travels, it would be desirable to have a personal, easily transportable
22 apparatus available which is operable for the iontophoretic transdermal delivery of a
23 medication packaged in a single dosage applicator. A problem which presents an
24 impediment to potential users is the necessity for reformulating medicaments for
25 iontophoretic delivery. Such reformulations must be approved by cognizant
26 regulatory agencies prior to sale. This requires delay and additional expense for the
27 manufacturer, which additional expense may be passed along to consumers. The
28 present invention provides a disposable medicament dispensing electrode for use with
29 a portable iontophoretic medicament delivery apparatus in which the electrode is
30 adapted for use with the apparatus for self-administering medicament. The

1 medicament dispensing portion of the electrode can accept, store and dispense
2 presently approved medicament formulations.

4 SUMMARY OF THE INVENTION

5 The present invention discloses a unit dosage medicament applicator electrode
6 adapted for use with a portable iontophoretic transdermal or transmucosal
7 medicament delivery apparatus for the self-administration of a unit dose of a
8 medicament into the skin. While the discussion to follow refers to iontophoretic
9 devices, it is understood that an ionosonic device is included within the meaning of
10 iontophoretic devices. The electrode and current supply apparatus is particularly
11 suited for the localized treatment of herpes infections. The established treatment for
12 recurrent genital herpetic lesions has been primarily supportive; including local topical
13 application of anesthesia. Severe cases have been treated with systemic Acyclovir®,
14 Zovirax® (Glaxo -Wellcome) or Famvir® (SmithKline Beecham). Some cases the
15 condition is managed with prophylactic long-term dosing administration with a
16 suitable antiviral agent at great expense. Systemic treatment of acute herpetic flare-
17 ups may reduce the normal 10-12 day course of cutaneous symptoms into a 6-8 day
18 episode. Topical treatment of lesions with Acyclovir® has not been as effective as in
19 vitro studies would suggest. A compound which is not presently available to clinicians
20 but has demonstrated significant anti herpetic activity is 5-iodo-2 deoxyuridine
21 (IUDR). Both of those agents have shown limited clinical efficacy when applied
22 topically to the herpetic lesion. It is the present inventor's contention that the limited
23 efficacy of topical administration previously observed is, at least in part, due to the
24 poor skin penetration of these medicaments when applied topically. The present
25 invention discloses a mesh-like iontophoresis electrode, which contains and dispenses
26 pre-approved formulations of those medicaments and provides improved transdermal
27 delivery of these medicaments. The device and associated medicament dispensing
28 electrodes may be used to treat such diverse conditions as herpes, warts, acne and
29 psoriasis.

30 Genital herpes (usually herpes simplex II infection) afflicts many people, cause
31 discomfort, shame, and may contribute to more severe and costly illnesses such as

1 cervical cancer, prostate cancer, and perinatal blindness from herpetic conjunctivitis.
2 Certain formulations containing anti-viral and/or anti-microbial drugs have been
3 approved for topical application by the cognizant regulatory agency. Reformulation
4 of such compositions for iontophoretic transdermal drug delivery entails significant
5 delays before such technology is available to the public for general use. The present
6 invention discloses a medicated iontophoresis electrode for the portable transdermal
7 delivery of Acyclovir® (9-[(2-hydroxyethoxy)methyl]guanine) or similar anti-viral
8 agent formulations which have already received (or may in the future receive)
9 regulatory approval to greatly benefit these afflicted patients. In a second preferred
10 embodiment of the invention, the medicament delivery electrode is attached to a user-
11 wearable glove having one or more fingers or merely a finger cot covering at least a
12 portion of one or more fingers of a user's hand.

13 It is an object of the present invention to provide an iontophoretic medicament
14 delivery electrode which is adapted to be used with an iontophoresis device operable
15 for self-administration of medicament into the skin of a person.

16 It is another object of the present invention to provide an improved
17 iontophoretic transdermal drug delivery apparatus having a medicament-containing
18 application electrode which dispenses and transdermally delivers a single dosage and
19 which is disposable and non-reusable.

20 It is a further object of the present invention to provide an iontophoresis
21 electrode meeting the above objectives which can receive and retain a previously
22 approved drug formulation for dispensation by ionosonic transdermal delivery.

23 It is still another advantage of the present invention to provide an improved
24 disposable iontophoretic medicament applicator which meets the above objectives and
25 which is inexpensive, safe to use and greatly increases the therapeutic efficacy of a
26 medicament administered thereby.

27 The medicament-containing electrode in accordance with the present
28 invention, together with an iontophoresis or ionosonic apparatus, provides a means
29 for transdermally administering medicament dispersed in a variety of previously
30 approved formulations directly and with high efficiency into a diseased tissue thereby
31 providing a novel method for treating clinical conditions presenting cutaneous and/or

-5-

1 mucocutaneous symptoms such as warts, acne, superficial fungus infections,
2 hyperproliferative diseases such as psoriasis, and particularly mucocutaneous Herpes
3 simplex viral eruptions and sequelae associated therewith.

4 The above objects, features and advantages of the invention are realized by the
5 improved iontophoretic medicament applicator electrode of the present invention. The
6 objects, features and advantages of the invention will become apparent upon
7 consideration of the following detailed disclosure of the invention, especially when it
8 is taken in conjunction with the accompanying drawings wherein:

11 BRIEF DESCRIPTION OF THE DRAWINGS

12 FIG. 1 is a top plan view of a first embodiment of the disposable iontophoretic
13 medicament containing applicator electrode adapted for attachment to an
14 iontophoresis handpiece wherein the medicament dispensing portion of the electrode
15 is an open mesh.

16 FIG. 2 is a side elevational view of a preferred embodiment of the disposable
17 non-reusable iontophoretic applicator electrode for use with an iontophoresis
18 handpiece adapted for self-administration.

19 FIG. 3 is a top plan view of the iontophoresis applicator electrode in
20 accordance with claim 2.

21 FIG. 4 is a horizontal cross-sectional plan view of an iontophoresis handpiece
22 adapted for use with the embodiments of the medicament dispensing applicator
23 electrode of the present invention shown in Figures 1 - 3.

24 FIG. 5 is a perspective view showing the applicator electrode of Figures 1 - 3
25 releasably affixed to an iontophoresis handpiece in accordance with Figure 4.

26 FIG. 6 shows a patient preparing to self-administer medicament to a treatment
27 site.

28 FIG. 7 is a top plan view of an embodiment of a medicament dispensing
29 applicator electrode having unitary construction and an open mesh medicament
30 dispensing portion similar to the embodiment shown in Figures 1 - 3 and adapted for
31 attachment to the skin of a patient.

-6-

1 FIG. 8 is a horizontal cross-sectional view of the applicator electrode of
2 Figure 7 taken along section line 8-8.

3 FIG. 9 is a bottom plan view of the applicator electrode of Figure 7.

4 FIG. 10 is a perspective view of an embodiment of an iontophoresis device
5 and a medicament dispensing applicator electrode adapted to be releasably affixed to a
6 finger of a patient wherein the medicament dispensing portion of the electrode is an
7 open mesh.

8 FIG. 11 is a perspective view of the iontophoresis device and applicator
9 electrode of Figure 10 wherein the thimble-like applicator electrode has been removed
10 from the patient's finger.

11 FIG. 12 is a partially cut-away view of the iontophoresis applicator electrode
12 of Figures 10 and 11 showing the relationship between the applicator electrode, an
13 insulating finger cot and a wrist-worn adaptation of the iontophoresis device shown in
14 Fig. 4.

15 FIG. 13 is a plan view of a glove embodiment of the applicator electrode in
16 accordance with the present invention having a large area for medicament delivery.

17 FIG. 14 is a perspective view of a patient using the glove embodiment of FIG.
18 13 to self-administer a medicament to a relatively large portion of skin underlying the
19 glove, as in, for example, the treatment of acne.

20 FIG. 15 is a schematic elevational view of a hand-held ionosonic handpiece
21 having an applicator electrode in accordance with the present invention attached
22 thereto.

23 24 DESCRIPTION OF THE PREFERRED EMBODIMENT

25 FIG 1 shows, in top plan view, a first preferred embodiment of the hand-held
26 iontophoretic transdermal medicament delivery apparatus of the present invention.
27 The first preferred embodiment of the iontophoretic medicament-containing
28 application electrode is shown at 10. The application electrode 10 is preferably
29 disposable and non-reusable. The electrode 10 is suitable, for example, for
30 transdermally delivering anti-viral agents such as Acyclovir® for the treatment of cold
31 sores or genital herpes. The applicator electrode 10 is adapted for use with an

-7-

1 iontophoresis handpiece such as the handpiece shown in Figures 4 and 5. In use, the
2 applicator electrode 10 is detachably affixed to a hand-held iontophoresis handpiece
3 40 which handpiece presents a first electrically conductive surface 41 and a second
4 electrically conductive surface 42. The handpiece 40 comprises a current driver 45
5 which receives an electrical voltage from a voltage multiplier 46 which is in electrical
6 communication with one electrode 47 of an electrical power source 48 such as a
7 battery. The other electrode 49 of the battery is in electrical communication with a
8 tactile electrode 42 on the surface of the handpiece 40 which electrode is, in use, in
9 contact with the skin of one or more fingers of a user. The electrical current from the
10 current driver 45 is conducted through a wire or conductive strip 44 to the first
11 electrically conductive surface 41. When the applicator electrode 10 is attached to the
12 handpiece 40, the current passes through the conductive applicator electrode to the
13 skin of the user, returning to the second electrically conductive element 42, or "tactile
14 electrode" to drive the medicament 23 through the mesh-like matrix material 12 and
15 into the user's skin. The medicament or treatment agent is contained within a viscous
16 fluid vehicle which, in turn, is contained within a plurality of cellular apertures 12a
17 comprising the mesh 12.

18 The applicator electrode 10 comprises a substantially flat elongate strip having
19 lateral ends extending from a central medicament dispensing portion 12. The central
20 medicament dispensing portion 12 is of mesh-like construction and has vertical cells
21 dimensioned to accommodate a viscous fluid within the confines of the cellular
22 structures. The viscous fluid contained within each of the plurality of cells 12a
23 includes a medicament (not shown) which is in a form suitable for transport under the
24 influence of an electrical current. The lateral ends of the applicator electrode 10 may
25 include a mesh-like tactile conductive portion 11 which contains an electrically
26 conductive gel therewithin. The applicator electrode 10 has a skin-facing surface 13
27 and a device-facing surface 14. One or a plurality of cells 12a form one or a plurality
28 of apertures between the upper skin-facing surface 13 and the lower device-facing
29 surface 14. The device-facing surface 14 may further include an adhesive layer 18
30 applied thereto suitable for releasably adhering the applicator electrode 10 to the
31 positive (anode) or negative (cathode) pole of a iontophoresis handpiece. The

1 positioning of the electrode's tactile conductive portion 11 on the surface of the
2 handpiece is such that tactile conductive portion 11 makes electrical contact with the
3 tactile electrode 42 on the handpiece. When the applicator electrode 10 is correctly
4 positioned on the handpiece, the medicament dispensing reservoir 12 is in electrical
5 communication with the electrically contacting element 41 on the handpiece. In
6 addition, one or more small magnets 15 disposed within the applicator electrode 10
7 may be positioned on the handpiece to activate a switch within said handpiece which
8 turns the handpiece on and/or off. The relatively narrow, flexible areas 16 on the
9 electrode 10 enable the applicator electrode 10 to be bent and formed around the
10 handpiece. Figure 2 shows a cross-sectional view of the applicator electrode 10 of
11 Figure 1 taken along section lines 2-2. The material 17 forming the structural portion
12 of the applicator electrode 10 is preferably a non-electrically conducting elastomer. A
13 bottom view of the applicator electrode 10 of Figures 1 and 2 is shown in Figure 3.

14 Figure 5 is a perspective view of the applicator electrode 10 attached to the
15 handpiece 40 in position for use. Figure 6 shows a patient preparing to use the
16 iontophoresis device for administering medicament to herpes lesions on the face. The
17 patient 60 grasps the tactile electrode 42 with a finger 61 to make electrical
18 communication therewith. The patient then touches the tip 12 of the applicator
19 electrode 10 to the lesion 63 thereby completing the electrical circuit and the resulting
20 current flow driving the medicament into the skin.

21 Turning next to Figure 7, a second preferred embodiment of a medicament
22 dispensing applicator electrode in accordance with the present invention is shown at
23 70. The centrally located medicament dispensing portion 71 has cells 72 therewithin
24 which cells provide an aperture between the upper surface 73 and the lower, skin-
25 contacting surface 74 of the electrode 70. The applicator electrode 70 is shown in
26 cross-section along section lines 8-8 in Figure 8. The central medicament dispensing
27 portion 71 of the electrode 70 is mesh-like in construction. A plurality of vertical cells
28 72 are molded within the elastomer strip comprising the applicator electrode to form
29 apertures which communicate between the upper surface 73 and the lower surface 74.
30 A fluid or semi-fluidic vehicle containing a medicament is placed within the cells 72
31 which cells are dimensioned to retain the medicament therewithin until an electrical

1 current is passed therethrough. An adhesive layer 75 is coated upon the lower surface
2 74 of the applicator electrode. The adhesive is chosen to be hypoallergenic,
3 biocompatible and to releasably affix the electrode 70 to the skin.

4 A bottom view of the applicator electrode 70 of Figures 7 and 8 is shown in
5 Figure 9. In use, the embodiment of the applicator electrode 70 shown in Figures 7 -
6 9 is affixed to the skin via the adhesive surface 75. The iontophoresis handpiece 40 is
7 grasped between the fingers of the patient such that the tactile electrode (42 in Fig. 5)
8 is in contact with at least one of the patient's fingers. The handpiece is then advanced
9 to the medicament dispensing portion 71 of the applicator electrode 70 until it makes
10 contact therewith. The circuit formed between the fingers grasping the tactile
11 electrode 42 portion of the handpiece 40 and the lesion is made through the mesh
12 surface of the medicament dispensing portion of the applicator electrode. Current
13 flows through the handpiece to the medicament dispensing electrode and into the skin
14 of the patient to return to the handpiece via the fingers and the tactile electrode to
15 close the circuit. As the current flows through the medicament dispensing electrode
16 the current drives the medicament into the skin of the patient.

17 Turning now to Figure 10, a thimble-like medicament dispensing applicator
18 electrode 100 is shown attached to a finger 105 of a patient. The applicator electrode
19 100 is in electrical communication with one pole (cathode or anode) of a wrist-worn,
20 bipolar iontophoresis device 101 by means of a wire 102. The bottom 106 or wrist-
21 facing, skin-contacting surface of the bipolar iontophoresis device 101 is the other
22 pole (anode or cathode) comprising a conductive electrode. The iontophoresis device
23 101 is releasably affixed to the wrist by means of a strap 103. The iontophoresis
24 device 101 may be constructed similarly to the iontophoresis handpiece 40 except that
25 the working electrode 41 is attached to the wire 102 and the tactile electrode 42
26 replaced with a conductive electrode 106 forming the skin-contacting portion of the
27 device 101 which is in contact with the wrist of the patient. The applicator electrode
28 100 is electrically isolated from the finger 105 by means of an insulating finger cot
29 104. Current from the iontophoresis device 101 passes through the conductive wire
30 102 to an inner electrically conductive thimble 110 (Figure 11) to which the wire is
31 conductively attached by means of solder. The electrically conductive thimble 110 has

1 an overlying silicone elastomeric thimble 111. The elastomeric thimble 111 is
2 homogenous in composition and has an upper surface 112 and a lower surface 113
3 which comprises a mesh 113a. The mesh 113a has integral therewith a plurality of
4 retaining cells 114 which cells extend between the electrically conductive thimble 110
5 and the lower surface 113 and are dimensioned to contain a medicament. In
6 operation, current from the iontophoresis device 101 passes through the wire 102 to
7 the electrically conductive thimble 110 of the applicator electrode. The voltage
8 applied to the surface of the electrically conductive thimble 110 drives medicament
9 contained within the cells 114 of the mesh 113 into the skin of a user's body. The
10 current passes through the user's body to the conductive electrode (not shown) which
11 comprises the wrist-facing portion of the iontophoresis device 101. The iontophoresis
12 device 101 preferably includes a power source, a voltage multiplier, a driver and an
13 on/off switch as shown in the handpiece 40, but reconfigured to be worn on the wrist.
14 An enlarged perspective view of the applicator electrode 100 overlying a finger cot is
15 shown in structural relationship in Figure 12.

16 The simple design is capable of retaining and dispensing existing medicament
17 formulations in various viscosities because the size of the retaining cells 72 in the
18 mesh portion of the electrode may be varied. The structural matrix of the applicator
19 electrode is a flexible, preferably hypoallergenic, nonelectrically-conductive material.
20 A suitable material is Silastic®, a silicone elastomer which is biocompatible, non-
21 conductive, flexible and possessing sufficient structural rigidity to contain
22 medicaments and a delivery vehicle within the retaining cells 114. Further, Silastic
23 silicone elastomer is inert so that medicaments will not oxidize or otherwise have their
24 chemical structures damaged. An electrode constructed from silicone elastomer has a
25 prolonged shelf-life, is soft and pleasant on contact, is hypoallergenic and sufficiently
26 flexible to adhere to any anatomical contour such as presented by a thimble. Such
27 anatomical plasticity is a key advantage to the foregoing design. Other polymers, such
28 as polyurethane, are suitable as well. A hydrated hydrophilic cotton layer (not shown)
29 may be interposed between the medicament dispensing portion 71 and the electrically
30 conductive surface 41 of the handpiece 40 to provide pretreatment hydration of the

1 medicament dispensing portion or the mesh may be hydrated by the patient
2 immediately prior to use.

3 With reference to the embodiment of an iontophoresis applicator electrode
4 shown in Figures 7 - 9, the electrode is easily manufactured using mold technology
5 wherein uncured silicone elastomer is either poured into a complementary mold or
6 pressure-mold injected. The lower surface 74 of the non-medicament dispensing
7 portion of the electrode is coated with skin adhesive. The medicament dispensing
8 portion 71 functions as a medicament reservoir and is preferably between 1mm and
9 4mm thick, depending upon the amount of medicament required to be stored in the
10 cells 72. The medicament-retaining cells 72, which are preferably a hexagonal, honey
11 comb-like structure, retain the medicament therein through their surface tension.
12 Hexagonal cells also lessen cross channel conductivity by means of their vertical
13 orientation. The size and geometry of these cells can vary. The smallest cells, for
14 instance, would be more suited to retaining liquid medicaments while the larger cells
15 are better adapted to retain ointment-based medicaments. Medium cells are more
16 suited to retaining and dispensing gel medicaments and lotions. The silicone walls of
17 the cells can be chemically modified to change the hydrophobic surface characteristics
18 thereof and further improve retention of specially formulated liquid medicaments. For
19 additional cell stability and retention capabilities, the skin-facing surface of the cells
20 can be covered with non-wicking, fibrous and porous materials commonly used in
21 electrodes. A composite or unitary construction from a single mold can be used
22 depending on production cost, it is inexpensive to manufacture and it offers both a
23 compartment for storage of existing formulations as well as a structural backbone for
24 the application electrode. The surface treatments of the retaining material bounding
25 each of the cells to create hydrophilic or hydrophobic surface effects depending on the
26 formulation to be utilized is well known in the art. An example of such technology is
27 disclosed, for example, in US patent 5,589,563. For ointments and hydrophobic
28 materials, silicone is preferred. For water or gel medicaments, surface treatment such
29 as doping the elastomeric cell surface with hydrophilic molecules can be of additional
30 benefit, as described herein. The embodiments disclosed herein present the following
31 advantages:

-12-

1 Inexpensive manufacture;
2 Use of either injection or pour molding production;
3 Use of composite sheet cutout assembly;
4 Anatomically conforming;
5 Elastomer surface modification for optimum retention of medicament;
6 Variable retaining cell size;
7 Variable retaining cell geometry;
8 Ability to utilize existing medicament formulations;
9 May use a cotton or (other hydrophilic matrix) layer for rapid pre-treatment
10 hydration.
11 May be used with single or multi-channel dispersive iontophoretic drivers; and
12 May be used with iontophoretic or ionosonic devices.
13 An embodiment of the present invention adapted for delivering medicament to
14 a large area of skin is shown in Figure 13. The iontophoresis electrode is contained
15 within a glove adapted to conform to and be worn upon a patient's hand. The glove
16 embodiment 130 of the iontophoresis drug delivery electrode comprises an
17 elastomeric glove 131 having a plurality of holes or open pores 132 in the palmar
18 surface 133 thereof. Underlying the palmar surface 133 and disposed within the glove
19 between the skin 134 and glove is an electrically insulating sheet 135 having an inner
20 surface 136 and an outer surface 137, both of which surfaces are coated with an
21 electrically conductive layer 138. The inner conductive layer 136 is, in use, in
22 electrical communication with the skin. The outer conductive layer 137 is in contact
23 with the interior surface of the glove and the pores 132. A medicament 139 capable
24 of iontophoretic transdermal delivery is contained within the pores. A bipolar power
25 source 140 has a working electrode 141 in electrical communication with the outer
26 conductive layer 137 coating the electrically insulating sheet 135, and a ground
27 electrode (not shown) which is in electrical communication with the inner conductive
28 layer coating the electrically insulating sheet. When the power source 140 is
29 energized, an electrical current flows between the inner conductive layer and the outer
30 conductive layer, which layers are separated by the electrically insulating sheet, via the
31 patient's skin. The polarity and amplitude of the current flowing through pores into

-13-

1 the user's skin facilitates entry of the medicament into the skin. The glove
2 embodiment, shown in use in Figure 14, is particularly useful for transdermally
3 delivering medicament to large areas of skin.

4 The advantages of a unitary iontophoresis electrode and a glove and finger cot
5 embodiment of an iontophoresis electrode for drug delivery have been presented. It is
6 noted that similarly constructed electrodes may be employed for non-invasively
7 collecting molecular species from the blood. For example, the mesh may be
8 impregnated with an electrically conductive gel. The polarity of the gel, with respect
9 to the skin, may be employed to transport blood components through the skin into the
10 gel where such components may be detected and/or quantitated. Such measurements
11 are useful for monitoring blood levels of compounds such as glucose or drugs.

12 The hand held iontophoretic device 40 (Figure 4) may be modified to include a
13 piezoelectric element operable for imparting ultrasonic vibrational motion to the
14 applicator electrode 12 to further facilitate transdermal delivery of certain
15 iontophoretically transportable compounds. A schematic view of such a modified
16 handpiece similar to the handpiece 40 of Figure 4 is shown at 150 in Figure 15. The
17 applicator electrode 160 includes all embodiments of the applicator electrode
18 described for the iontophoresis handpiece discussed above. One side of an annular
19 ultrasonic piezoelectric element 151 is disposed rearwardly to the applicator electrode
20 160 containing a medicament. Power is supplied to energize the piezoelectric element
21 151 by means of conductive elements 157 and 152 which are in electrical
22 communication with an ultrasonic driver 163. An optional current sensitive switching
23 element (not shown) may be used to energize the piezoelectric element only when
24 current passes through the applicator electrode circuit. The applicator electrode 160
25 may include any applicator electrode heretofore described for use with an
26 iontophoretic handpiece. The applicator electrode 160 may contain an ionic
27 medicament or a biologically inactive ionic solution which penetrates the skin and
28 opens clogged pores under the influence of iontophoretically driven transport assisted
29 by ultrasonic waves in the cutaneous tissue. Stephen et al. have shown in US Patent
30 4,979,938 that the iontophoretic delivery of hydroxyl ions into the skin can be used to
31 treat acne. The ionosonic delivery of a similar anion may provide improved opening

-14-

1 of pores in the skin for treating acne. The combination of iontophoretic delivery of a
2 compound into a tissue, together with inducing ultrasonic vibration in the tissue, may
3 enable the removal of coloration (such as a blemish, freckle or tattoo) within the skin
4 by the delivery of a suitable bleaching agent

5 While the invention has been described above with references to specific
6 embodiments thereof, it is apparent that many changes, modifications and variations in
7 the materials, arrangements of parts and steps can be made without departing from the
8 inventive concept disclosed herein. For example, an impregnated conductive gel can
9 also be used to as medicament containing medium to increase the physical stability and
10 the tissue adhering characteristics of the electrode. The applicator electrode described
11 herein, when used with an ionosonic or iontophoretic handpiece can deliver
12 medicaments for treating diverse medical conditions including, but not limited to acne,
13 hyperproliferative diseases of the skin, superficial fungal infections, warts, and herpes
14 type viral infections. Accordingly, the spirit and broad scope of the appended claims
15 is intended to embrace all such changes, modifications and variations that may occur
16 to one of skill in the art upon a reading of the disclosure. All patent applications,
17 patents and other publication cited herein are incorporated by reference in their
18 entirety.

19
20 What I claim is:

CLAIMS

1
2
3 1. A medicament dispensing applicator electrode adapted for use with an
4 iontophoresis device comprising a unitary strip consisting of an elastomeric substrate
5 having an upper surface and a lower surface, said strip having a medicament
6 dispensing portion comprising a cell or a plurality of cells forming an aperture or a
7 plurality of apertures between said upper surface and said lower surface and wherein
8 said cell or plurality of cells contain a medicament.

9 2. The applicator electrode of Claim 1 further comprising a layer of
10 adhesive covering at least a portion of said upper surface of said strip, said adhesive
11 layer being operable for releasably attaching said strip to an iontophoresis device.

12 3. The applicator electrode of Claim 1 further comprising a layer of
13 adhesive covering at least a portion of said lower surface of said strip, said adhesive
14 layer being operable for releasably attaching said strip to skin.

15 4. The applicator electrode of Claim 2 further comprising a tactile
16 conductive portion having a second cell or a plurality of cells electrically insulated
17 from said medicament dispensing portion, said second cell or plurality of cells
18 containing an electrically conductive fluid.

19 5. The applicator electrode of Claim 3 further comprising a tactile
20 conductive portion having a second cell or plurality of cells electrically insulated from
21 said medicament dispensing portion, said second cell or plurality of cells containing an
22 electrically conductive fluid.

23 6. An iontophoresis device comprising, in combination:

24 (a) a current source having an anode and a cathode and a source of
25 electrical power; and

26 (b) the medicament dispensing applicator electrode of claim 4 wherein said
27 medicament dispensing portion of said applicator electrode is in electrical connection
28 with either of said anode or said cathode and said tactile conductive portion is in
29 electrical connection with either of said cathode or said anode, respectively.

30 7. A medicament dispensing iontophoresis applicator electrode
31 comprising a generally thimble-shaped electrically conductive member and an

1 overlying medicament dispensing portion of an electrically non-conducting elastomer
2 having a cell or plurality of cells in at least a portion thereof and wherein said thimble-
3 shaped conductive portion is dimensioned to fit over and conform to the shape of the
4 distal end of a finger.

5 8. The applicator electrode of Claim 7 wherein said cell or plurality of
6 cells contain a medicament.

7 9. The applicator electrode of Claim 8 further comprising an electrically
8 insulating layer underlying said thimble-shaped electrically conductive member.

9 10. The applicator electrode of Claim 8 wherein said thimble-shaped
10 electrically conductive member has a first end of an electrically conductive wire
11 affixed thereto.

12 11. The applicator electrode of Claim 10 wherein said electrically
13 conductive wire has a second end in opposition to said first end and includes means
14 for attaching said second end to a pole of a current source.

15 12. The applicator electrode of claim 8 wherein said medicament
16 dispensing portion further comprises a hydrophilic matrix layer overlying said cell or
17 plurality of cells for pre-treatment hydration by a user immediately prior to use when
18 used with non-ionic medicament formulation.

19 13. The applicator electrode of claim 12 wherein said hydrophilic matrix
20 layer is hydrated.

21 14. A method for treating lesions associated with cold sore and genital herpes
22 comprising the steps of:

23 (a) presenting a hand-held iontophoretic device comprising an electrode
24 and a medicament dispensing reservoir containing an antiviral agent, said reservoir
25 being in electrical communication with said electrode of the iontophoretic device; and

26 (b) bringing the medicament dispensing reservoir into contact with said
27 lesions; then

28 (c) applying a voltage gradient between the electrode and the lesion.
29

1

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3 15. The method of claim 14 wherein said medicament comprises
4 (2 amino-1, 9-dihydro-9-[(2-hydroxyethoxy) methyl]-6H-purin-6-one) or
5 iontophoretically transportable analogs thereof.

6 16. A method for treating lesions associated with cold sore and genital
7 herpes comprising the steps of:

8 (a) presenting a hand-held ionosonic device comprising an electrode and a
9 medicament dispensing reservoir containing an antiviral agent, said reservoir being in
10 electrical communication with said electrode; and

11 (b) bringing the medicament dispensing reservoir into contact with said
12 lesions; then

13 (c) inducing ultrasonic vibration in a tissue comprising the lesion; and

14 (d) applying a voltage gradient between the electrode and the lesion.

15 17. The method of claim 16 wherein said medicament comprises (2 amino-
16 1, 9-dihydro-9-[(2-hydroxyethoxy) methyl]-6H-purin-6-one) or ionosonically
17 transportable analogs thereof.

18 18. A method for treating lesions associated with acne comprising the
19 steps of:

20 (a) presenting a hand-held ionosonic device comprising an electrode and a
21 medicament dispensing reservoir containing an ionic compound in electrical
22 communication with said electrode; and

23 (b) bringing the medicament dispensing reservoir into contact a said lesion;
24 then

25 (c) inducing ultrasonic vibration in a tissue comprising the lesion; then

26 (d) applying a voltage gradient between the electrode and the lesion

27 19. The method of claim 18 wherein said ionic compound is anionic.

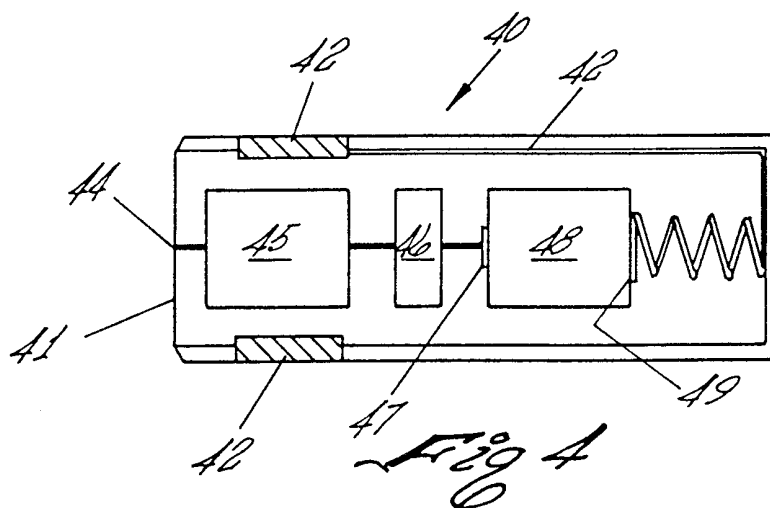
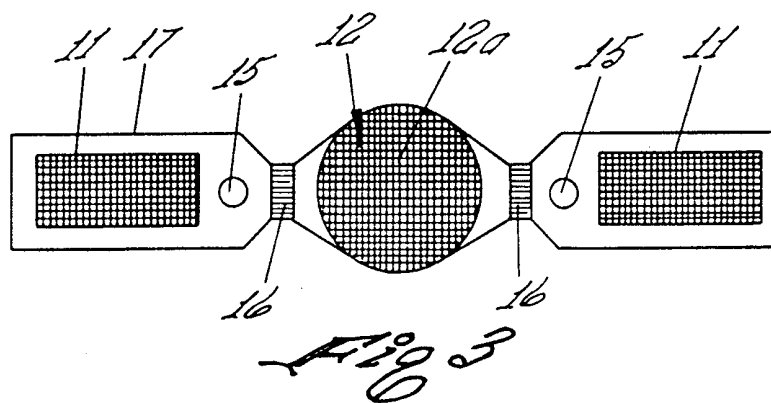
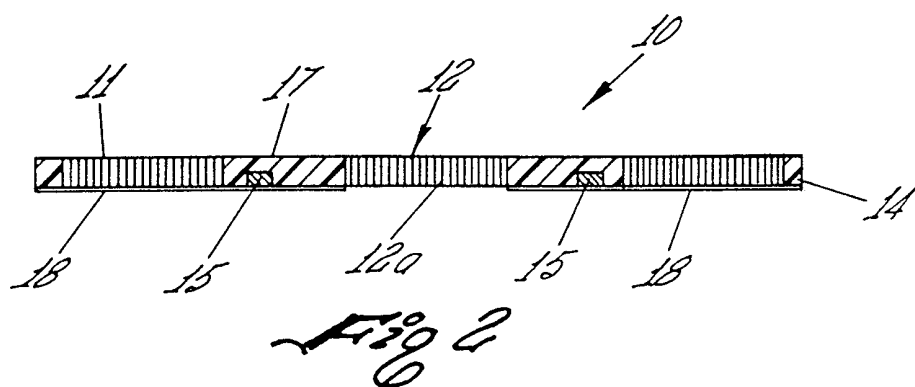
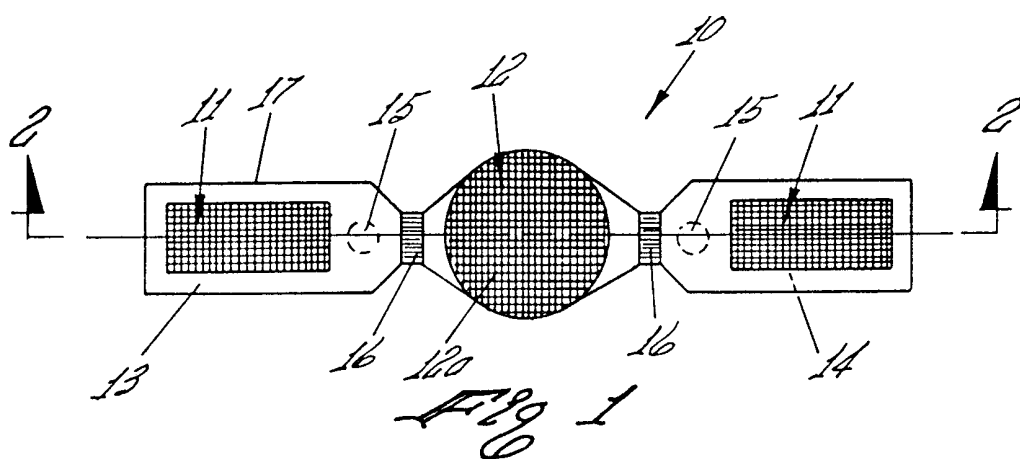
1 20. The method of claim 18 wherein said ionic compound is a
2 hydroxyl ion.

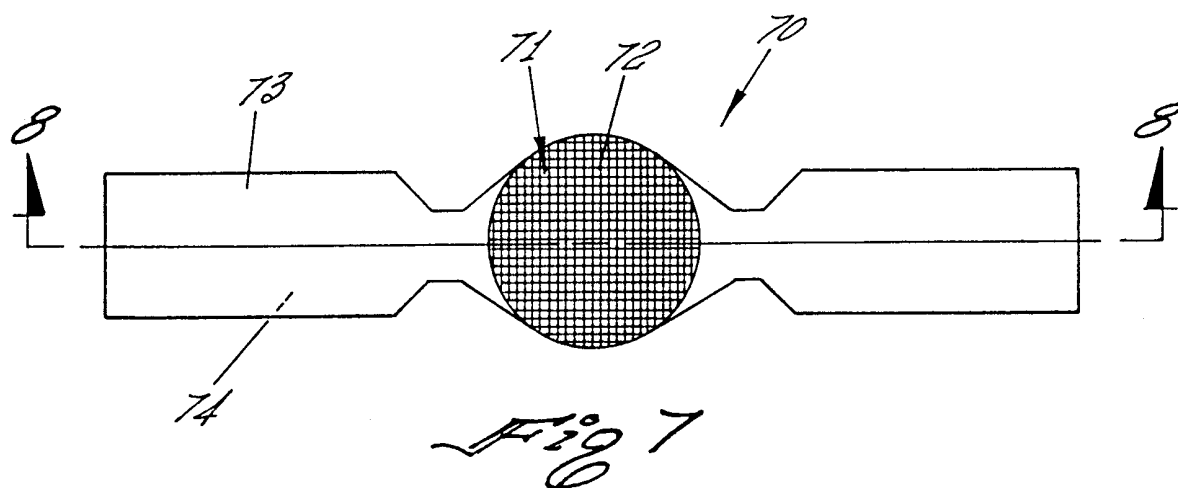
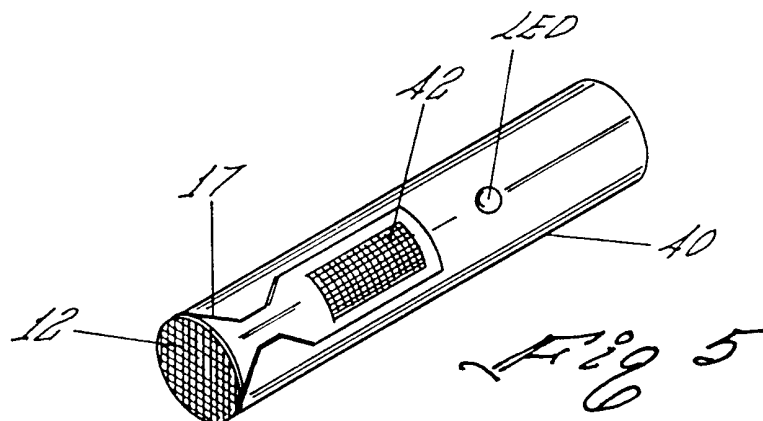
3 21. The method of claim 18 wherein said ionic compound is cationic.
4

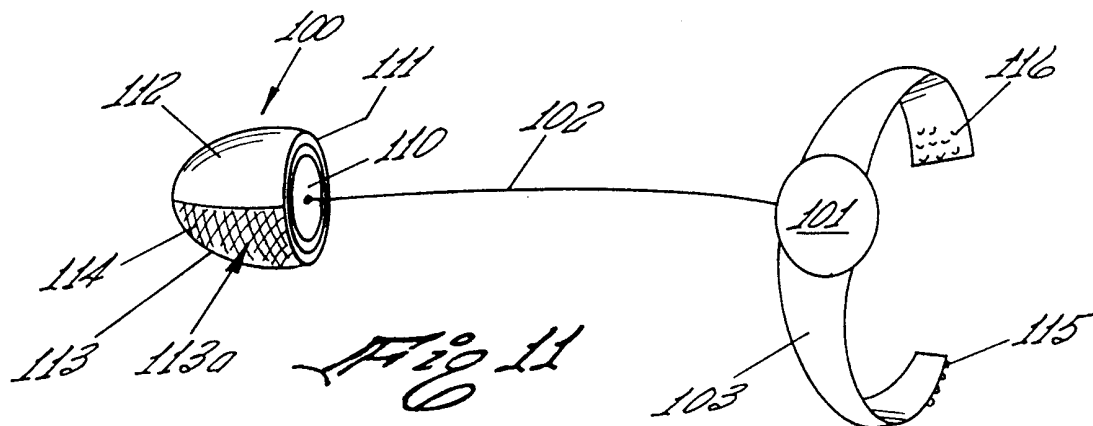
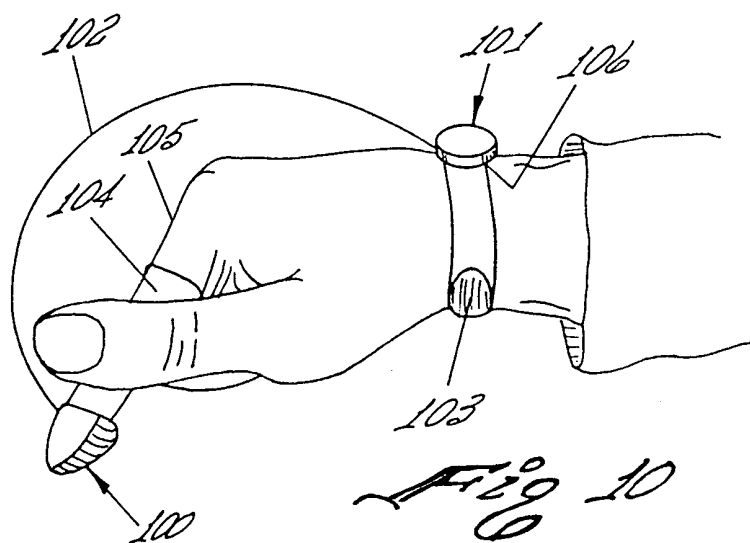
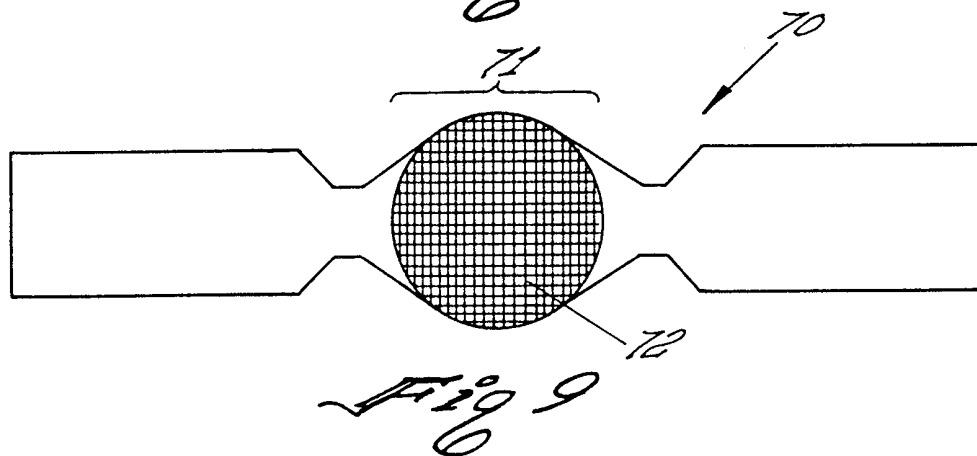
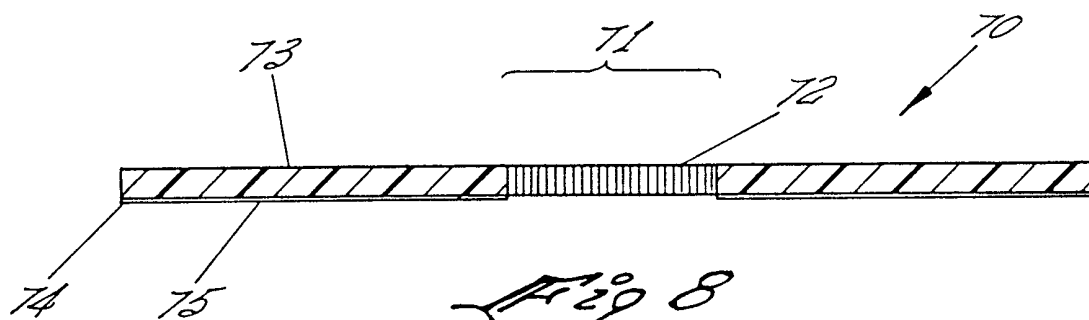
5 22. A disposable medicament dispensing applicator electrode for an
6 iontophoretic drug delivery device adapted for the self-administration of a medicament
7 into a person's skin, said device comprising a base assembly having an active terminal
8 adapted to receive and make electrical contact with a detachable medicament
9 dispensing applicator electrode wherein said base assembly comprises; a case having
10 an elongate, substantially cylindrical outer surface having a size and shape adapted to
11 be comfortably grasped within a person's hand and wherein at least a portion of said
12 outer surface is a tactile electrode formed of an electrically conductive material; and a
13 bipolar electrical power means having a first pole and a second pole; said electrical
14 power means being enclosed within said case and wherein said first pole is in electrical
15 communication with said tactile electrode; wherein said medicament dispensing
16 applicator electrode comprises: a module containing unit dose of medicament, an
17 electrically conductive working electrode and means thereon adapted for releasably
18 attaching said working electrode to said second pole of said electrical power means
19 wherein said working electrode further comprises an elongate strip constructed of a
20 substantially electrically non-conductive substrate material, said strip having a central
21 portion containing a medicament in an electrically conductive substrate and laterally
22 symmetric end portions having cutouts therewithin.

23 23. The disposable medicament dispensing applicator electrode of claim 22
24 wherein said cutouts in said laterally symmetric end portions contain an electrically
25 conductive material.

26 24. The disposable medicament dispensing applicator electrode of claim 23
27 wherein said electrically conductive material is a gel.







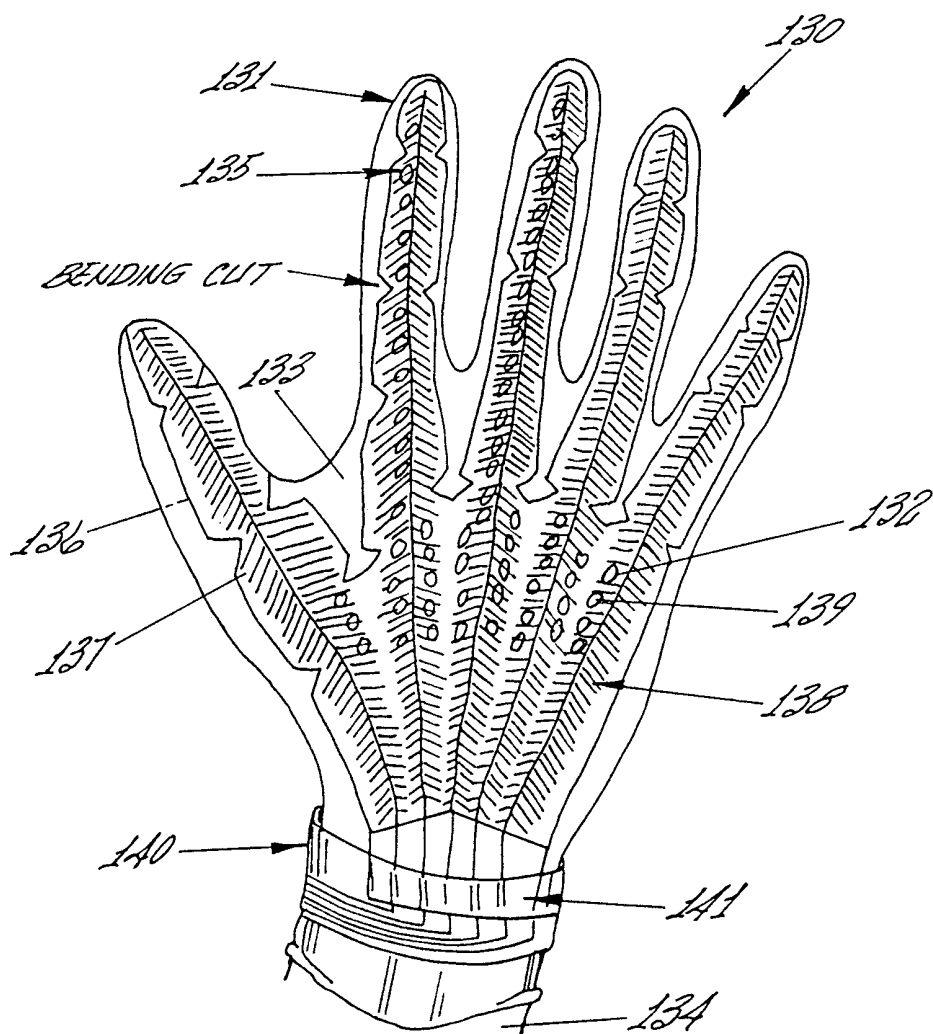
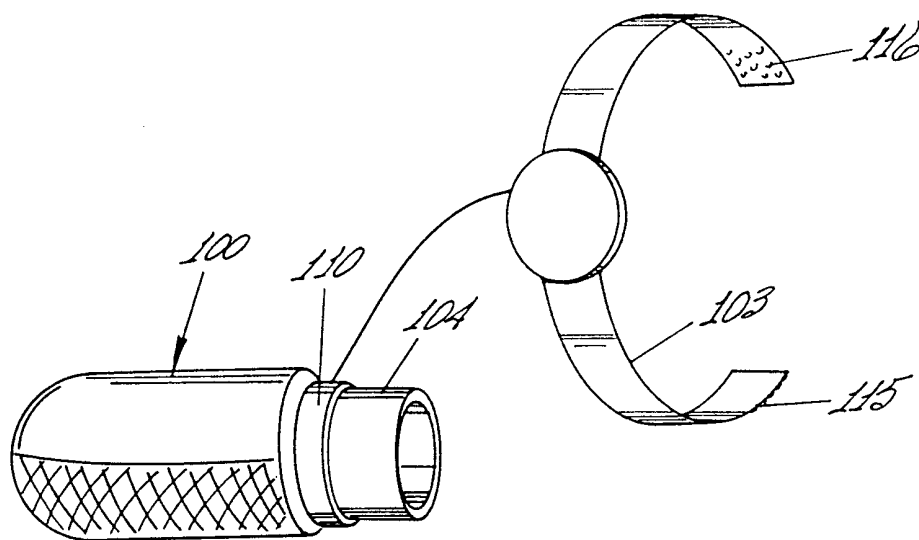




Fig 14

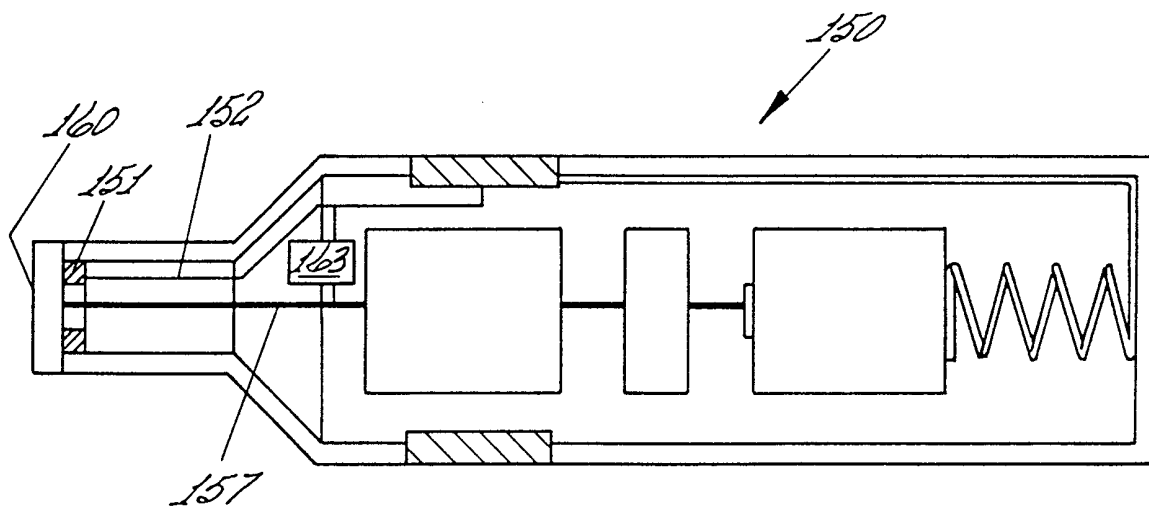


Fig 15

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US99/11440

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) :A61B 17/20; A61M 31/00; A61N 1/30

US CL :604/20, 22, 501

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 604/19- 20, 22, 48, 501; 607/75, 111, 145

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 279,524 A (BEATY) 19 June 1883, all.	7-13
A	US 3,163,166 A (BRANT et al.) 29 December 1964, all.	22
A	US 4,838,273 A (CARTNELL) 13 June 1989, col. 4 line 3 to col. 5 line 5.	1-13, 22
A	US 4,953,565 A (TACHIBANA et al.) 04 September 1990, all.	16, 18
X	US 5,458,569 A (KIRK, III et al.) 17 October 1995, Figs. 5 and 6, col.3 line 42 to col. 7 line 30.	1-6
A	US 5,658,247 A (HENLEY) 19 August 1997, all.	1-24

☒ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

* Special categories of cited documents:	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"A" document defining the general state of the art which is not considered to be of particular relevance	"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"E" earlier document published on or after the international filing date	"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"&" document member of the same patent family
"O" document referring to an oral disclosure, use, exhibition or other means	
"P" document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

28 JUNE 1999

Date of mailing of the international search report

08 JUL 1999

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INTERNATIONAL SEARCH REPORT

International application No.
PCT/US99/11440

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5,676,648 A (HENLEY) 14 October 1997, all.	1-24
A, P	US 5,879,323 A (HENLEY) 09 March 1999, all.	1-24